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Full Length Research Paper

# Peristaltic transport of micropolar fluid through porous medium in a symmetric channel with heat and mass transfer in the presence of generation and radiation

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The effect of heat generation and radiation on the peristaltic motion of micropolar fluid with heat and mass transfer through porous medium in a symmetric channel was investigated. The equations of motion for micropolar fluids were introduced as well as the equations of energy and concentration. The system of these equations written in two dimensions and then transformed using the transformations between a laboratory and fixed frames. The yield equations were solved analytically with the appropriate boundary conditions under the approximation of low Reynolds number and long wavelength. The longitudinal velocity, the microrotation velocity, the temperature and the concentration are plotted and shown graphically and discussed for different physical parameters of the problem.

**Key words:** Peristaltic transport, micropolar fluid, porous medium, heat and mass transfer, heat generation, thermal radiation, thermal diffusion.

### INTRODUCTION

Peristalsis is defined as a wave of relaxation contraction (expansion) imparted by the walls of a flexible conduit, thereby pumping the enclosed material, it is a nature's way of moving the content within hollow muscular structures by successive contraction of their muscular fibers (Eytan et al., 2001; Fung and Yih, 1968; Mishra and Rao, 2003; Mekheimer, 2003). Peristalsis is now well-known to the physiologists to be one of the major mechanisms for fluid transport in many biological systems, as it results physiologically from neuron muscular properties of the tubular smooth muscles (Srivastava and Srivastava, 1982; El-Shehawey et al., 2006; Gharsseldien et al., 2010; Gharsseldien, 2003).

The peristaltic transport may be involved in many biological organs, for instance, moving food through the esophagus; movement of chime in the gastrointestinal tract; urine transport from the kidney to the bladder through the ureter; transport of spermatozoa in the ducts efferents of male reproduction tract and in the cervical canal of the female; movement of ova in the fallopian tub; vasomotion of small blood vessels such as venules and capillaries as well as blood flow in arteries, and in many other glandular ducts (EI-Shehawey et al., 2006; EI-Shehawey and Husseny, 2000; Mekheimer, 2003; Mishra and Rao, 2003; Srivastava and Srivastava, 1982). There are also many industrial applications of the peristaltic transport like, blood pumps in heart lung machine, transport of corrosive fluid, where the contact of the fluid with the machinery parts is prohibited (Mishra and Rao, 2003).

The theory of microfluid introduced by Eringen, deals with a class of fluids which exhibit certain microscopic



Figure 1. The geometry of the problem.

effects arising from the local structure and micro-motions of the fluid elements. A subclass of these fluids is the micropolar fluids, like blood, liquid crystals and polymers, can support couple stresses, body couples and exhibit micro-rotational and micro-inertial effects. Eringen is the first researcher who put out the theory to find a mathematical model of the micropolar fluids (Eringen, 1966). These equations are a generalization of the (Newtonian) Navier-Stokes equations and deals with three fields: velocity vector  ${\bf V}$ , the pressure of the fluid

P and microrotation vector  $\mathbf{W}$ , together with some viscosity parameters and material constants to describe the behavior of the fluid (Eldabe et al., 2008 and El-Sayed et al., 2011). Some researchers attempted studying the peristaltic flow problems concerning the micropolar fluids, (Ali and Hayat 2008; Devi and Devanathan, 1975; Hayat and Ali, 2008; Hayat et al., 2007; Mekheimer and Abd Elmaboud, 2008; Muthu et al., 2003, 2008; Srinivasacharya et al., 2003) and others studied the heat transfer effect with peristalsis or not for different fluids (Abo-Eldahab et al. 2012; Eldabe, 2001; Eldabe et al., 2008; Eldabe and Mohamed, 2002; El-Sayed et al., 2011; Hayat and Hina, 2010; Nadeem and Noreen 2009; Nadeem et al., 2010).

In the current study we investigated the effects of heat generation and radiation with heat and mass transfer on peristaltic transport of micropolar fluid through porous medium in a symmetric channel.

#### **Basic equations**

After studying the motion of micropolar fluid through porous medium with heat and mass transfer, the basic equations which describe this motion can be written as: Continuity equation

$$\frac{\partial \rho}{\partial t} + \nabla \cdot (\rho \mathbf{V}) = 0, \tag{1}$$

Conservation of liner momentum

$$\rho \mathbf{V} = (\lambda_{\nu} + 2\mu_{\nu} + k_{\nu})\nabla(\nabla \cdot \mathbf{V}) - (\mu_{\nu} + k_{\nu})\nabla \times \nabla \times \mathbf{V} + k_{\nu}\nabla \times \mathbf{w} - \nabla P - \frac{(\mu_{\nu} + k_{\nu})}{k}\mathbf{V}$$
(2)

Conservation of angular momentum

$$\rho \mathbf{j} \mathbf{w} = (\alpha_{\nu} + \beta_{\nu} + \gamma_{\nu}) \nabla \nabla \cdot \mathbf{w} - \gamma_{\nu} \nabla \times \nabla \times \mathbf{w} + k_{\nu} \nabla \times \mathbf{V} - 2k_{\nu} \mathbf{w} + \rho \mathbf{l},$$
(3)

Heat equation

$$\rho c_p \frac{dT}{dt} = k_1 \nabla^2 T + Q(T - T_0) - \nabla \cdot q_r, \qquad (4)$$

Concentration equation

$$\frac{dC}{dt} = D_m \nabla^2 C + D_m k_T \nabla^2 T,$$
(5)

where **V** is the velocity vector of the fluid,  $\mathbf{w} = (0,0,w)$  is the microrotation vector, k is the permeability of porous medium, 1 is the body couple,  $\rho$  is the fluid density, j is the microinertia parameter, T is temperature,  $^{C_p}$  is the specific heat at constant pressure,  $q_r$  is the radiation heat flux vector,  $k_1$  is the thermal conductivity, Q is heat generation, C is the concentration,  $^{D_m}$  is the coefficient of mass diffusivity,  $k_T$  is the thermal diffusion ratio and  $^{\alpha_v}$ ,  $^{\beta_v}$ ,  $^{\gamma_v}$ ,  $^{\lambda_v}$ ,  $^{\mu_v}$ and  $^{k_v}$  are the material parameters (Eringen, 1966) (different viscosities that characterize the isotropic properties of the fluid), satisfy

$$2\mu_{\nu} + k_{\nu} \ge 0, \qquad k_{\nu} \ge 0, \qquad 3\alpha_{\nu} + \beta_{\nu} + \gamma_{\nu} \ge 0, \qquad \gamma_{\nu} \ge |\beta_{\nu}|.$$
(6)

#### Mathematical formulation

Consider that the micropolar fluid moves in two-dimensions of cartesian coordinates  $^{(X,Y)}$ , where X-axis is taken in motion direction while Y-axis is perpendicular on it and  $^{(U,V)}$  are the velocity components in X and Y directions respectively as shown in Figure 1. Neglecting body couple, with solenoidal microrotation vector, then the previous equations of become:

$$\frac{\partial U}{\partial X} + \frac{\partial V}{\partial Y} = 0, \tag{7}$$

$$\rho\left(\frac{\partial U}{\partial t} + U\frac{\partial U}{\partial X} + V\frac{\partial U}{\partial Y}\right) = (\mu_{\nu} + k_{\nu})\nabla^{2}U + k_{\nu}\frac{\partial w}{\partial Y} - \frac{\partial P}{\partial X} - \frac{(\mu_{\nu} + k_{\nu})}{k}U, \quad (8)$$

$$\rho\left(\frac{\partial V}{\partial t} + U\frac{\partial V}{\partial X} + V\frac{\partial V}{\partial Y}\right) = (\mu_{\nu} + k_{\nu})\nabla^{2}V - k_{\nu}\frac{\partial w}{\partial X} - \frac{\partial P}{\partial Y} - \frac{(\mu_{\nu} + k_{\nu})}{k}V, \quad (9)$$

$$\rho j \left( \frac{\partial w}{\partial t} + U \frac{\partial w}{\partial X} + V \frac{\partial w}{\partial Y} \right) = \gamma_{\nu} \nabla^2 w + k_{\nu} \left( \frac{\partial V}{\partial X} - \frac{\partial U}{\partial Y} \right) - 2k_{\nu} w,$$
(10)

$$\rho c_{p} \left( \frac{\partial T}{\partial t} + U \frac{\partial T}{\partial X} + V \frac{\partial T}{\partial Y} \right) = k_{1} \left( \frac{\partial^{2} T}{\partial X^{2}} + \frac{\partial^{2} T}{\partial Y^{2}} \right) - \left( \frac{\partial q_{r}}{\partial Y} \right) + Q(T - T_{0}),$$
(11)

$$\left(\frac{\partial C}{\partial t} + U\frac{\partial C}{\partial X} + V\frac{\partial C}{\partial Y}\right) = D_m \left(\frac{\partial^2 C}{\partial X^2} + \frac{\partial^2 C}{\partial Y^2}\right) + D_m k_T \left(\frac{\partial^2 T}{\partial X^2} + \frac{\partial^2 T}{\partial Y^2}\right).$$
(12)

Using the Rosselent approximation we  $q_r = -\frac{4}{3} \frac{\sigma_0}{k_0} \frac{\partial T^4}{\partial Y}_{\text{where }} \sigma_0$  is the Stefan-Boltzmann  $k_0$ 

constant and  $k_0$  is the mean absorption coefficient (Mahmoud and waheed, 2012).

The geometry of the wall surface is defined as

$$Y = H = d + b\cos\frac{2\pi}{\lambda}(X - ct),$$
(13)

where d is the half-width of the channel, b is the wave amplitude,  $\lambda$  is the wavelength, c is the velocity propagation, and t is the time. The appropriate boundary conditions are:

$$\psi = 0, \quad \frac{\partial^2 \psi}{\partial Y^2} = 0, \quad w = 0, \quad T = T_o, \quad C = C_0 \quad at \ Y = 0,$$
 (14)

$$\psi = q, \quad w = \frac{-\alpha}{2} \left( \frac{\partial V}{\partial X} - \frac{\partial U}{\partial Y} \right), \quad \frac{\partial \psi}{\partial Y} = 0, \quad T = T_w, \quad C = C_w \quad at \ Y = H,$$
(15)

where  $\psi$  is the stream function ( $U = \frac{\partial \psi}{\partial Y}$  and  $V = -\frac{\partial \psi}{\partial X}$ ) q is the flux of flow and

 $\partial Y$   $\partial X$ , q is the flux of flow, and according to Bayada and Banhaoucha (2008), it is proposed to link the value of the microrotation value with the rotation of the velocity by way of a coefficient  $\alpha$ ,

$$\mathbf{w} \times \mathbf{n} = \frac{\alpha}{2} (\nabla \times \mathbf{V}) \times \mathbf{n}, \tag{16}$$

where  ${f n}$  is the normal unit vector on the boundary, lpha characterizes the microrotation on the solid surfaces and its value is

evaluated by the relation:

$$0 \le \alpha \le \frac{\mu_{\nu} + k_{\nu}}{k_{\nu}}.$$

Introducing a wave frame (x, y) moving with the velocity  $^{C}$  away from the laboratory frame (X, Y), by the transformations

$$x = X - ct, \quad y = Y, \quad u = U - c, \quad v = V, \quad p(x) = P(X, t),$$
 (17)

where u and v are the fluid velocity components and p is pressure in the wave frame of references. Further, we introduce the following non-dimensional variables:

$$\overline{x} = \frac{x}{\lambda}, \quad \overline{y} = \frac{y}{d}, \quad \overline{u} = \frac{u}{c}, \quad \overline{v} = \frac{v}{c\delta}, \quad h = \frac{H}{d}, \quad \delta = \frac{d}{\lambda},$$

$$\overline{\psi} = \frac{\psi}{c d}, \quad \overline{p} = \frac{d^2 p}{\mu \lambda c}, \quad R_e = \frac{\rho c d}{\mu}, \quad \overline{j} = \frac{j}{d^2},$$

$$\overline{w} = \frac{wd}{c}, \quad k = \frac{d^2}{K^2}, \quad \Theta = \frac{T - T_0}{T_w - T_0}, \quad \Phi = \frac{C - C_0}{C_w - C_0}.$$
 (18)

After using transformation (17), dimensionless variables (18), after dropping bars and under the assumptions of long wave length ( $\delta \ll 1$ ) and low Reynolds number ( $^{R_e}$ ), the Equations 7 to 12 becomes:

$$\frac{\partial p}{\partial x} = \left(\frac{1}{1-N}\right)\frac{\partial^2 u}{\partial y^2} + \left(\frac{N}{1-N}\right)\frac{\partial w}{\partial y} - \left(\frac{1}{K(1-N)}\right)(u+1),$$
(19)

$$\frac{\partial p}{\partial y} = 0,$$
(20)

$$\left(\frac{2-N}{\beta^2}\right)\frac{\partial^2 w}{\partial y^2} - \frac{\partial u}{\partial y} - 2w = 0,$$
(21)

$$\left(1 + \frac{4}{3}\frac{1}{R_n}\right)\frac{\partial^2\Theta}{\partial y^2} + P_r G\Theta = 0,$$
(22)

$$\frac{1}{S_c}\frac{\partial^2 \Phi}{\partial y^2} + S_r \frac{\partial^2 \Theta}{\partial y^2} = 0$$
(23)

also, the channel wall equation will be :

$$y = h = 1 + \phi \cos 2\pi x, \tag{24}$$



**Figure 2.** The velocity profile u against y for different values of coupling number N when:  $\phi = 0.5$ , x = 1,  $\alpha = 1$  $K = 1.5 \quad \beta = 5 \quad q = 1$ 

where 
$$N = \frac{k_{\nu}}{\mu_{\nu} + k_{\nu}}$$
 is the coupling number  $(0 \le N \le 1)$ ,  

$$\beta^{2} = \frac{k_{\nu}d^{2}(2\mu_{\nu} + k_{\nu})}{\gamma_{\nu}(\mu_{\nu} + k_{\nu})}$$
 is the micropolar parameter,  

$$P_{r} = \frac{\mu_{\nu}C_{p}}{k_{\nu}}$$

$$R_{r} = \frac{k_{1}k_{0}}{k_{0}}$$

$$R_r = \frac{R_n}{k_1}$$
 is the Prantdel number,  $R_n = \frac{1}{4\sigma_0 T_0^3}$  is the radiation

$$G = \frac{Qd}{d}$$

 $\overline{\mu_{v}C_{p}}$  is parameter, the generation parameter,  $S_{r} = \frac{\rho D_{m} k_{T} (T_{w} - T_{0})}{\mu_{v} (C_{w} - C_{0})}$  $S_c = rac{\mu_v}{
ho D_m}$  is the is the Soret number,

> <1 d

is the amplitude ratio. Schmidt number and Using Equation (20) into (19), the previous Equations (in terms of stream function, will be:

$$\psi_{yyyy} + Nw_{yy} - \frac{1}{K}\psi_{yy} = 0,$$
 (25)

$$\psi_{yy} - \left(\frac{2-N}{\beta^2}\right) w_{yy} + 2w = 0,$$
 (26)

$$\left(1 + \frac{4}{3}\frac{1}{R_n}\right)\frac{\partial^2\Theta}{\partial y^2} + P_r G\Theta = 0,$$
(27)

$$\frac{1}{S_c}\frac{\partial^2 \Phi}{\partial y^2} + S_r \frac{\partial^2 \Theta}{\partial y^2} = 0$$
(28)

Also, we can write down the non-dimensional boundary conditions in terms of the stream function as follows:

$$\psi = 0, \qquad \psi_{yy} = 0, \qquad w = 0, \quad \Theta = 0, \quad at \ y = 0,$$
 (29)

$$\psi = q, \quad w = \frac{-\alpha}{2} \psi_{yy}, \quad \psi_{y} = -1, \quad \Theta = 1, \quad at \ y = h,$$
(30)

Introducing these conditions into the general solutions of the Equations (25-28), the solutions of the stream function and the microrotation velocity, temperature and concentration respectively are given by:

$$\psi = \frac{L_1 y + L_2 \sinh(y\gamma_1) - L_3 \sinh(y\gamma_2)}{L_4}$$
(31)

$$w = \frac{L_5 \sinh(y\gamma_1) + L_6 \sinh(y\gamma_2)}{L_7}$$
(32)

$$\theta = \operatorname{csch}(h\gamma_3)\sinh(y\gamma_3) \tag{33}$$

$$\phi = \left(\frac{S_c S_r + 1}{h}\right) y - S_c S_r csch(h\gamma_3) \sinh(y\gamma_3)$$
(34)

where  $\gamma_i (i = 1, 2, 3)$  ,  $L_j (j = 1, ...7)$  and  $n_k (k = 1, ...18)$ are given in the appendix.

#### **RESLUTS AND DISCUSSION**

In the present study, the problem of peristaltic transport of micropolar fluid under the effects of heat generation and radiation with heat and mass transfer through a symmetric channel is modeled mathematically. The governed equations of this problem are formed in two dimensions and transformed from a laboratory frame to a fixed frame, the yield equations written in dimensionless form. The analytical solutions of these equations have been obtained under the conditions of low Reynolds number and long wave length, subject to a set of appropriate boundary conditions using the Mathematica Program. The expressions of velocity profile, microrotation velocity, temperature and concentration distributions have been evaluated for different physical parameters of the problem and have been shown graphically through a set of figures. In our figures we chose y between 0 and 1.5 we observed that in the region  $0 \le y \le 0.8$ 

Figure 2 explained the effect of coupling number N on the velocity u, it is observed that u decreases with increasing of N and after that, the velocity profile



Figure 3. The velocity profile  $^{u}$  against  $^{y}$  for different values of K when:  $\phi = 0.5$ , x = 1,  $\alpha = 1$ , N = 0.1,  $\beta = 5$ , q = 1



Figure 4. The microrotation  ${}^{W}$  against  ${}^{Y}$  for different values of coupling number N when:  $\phi = 0.5$ , x = 1,  $\alpha = 0$ , K = 1.5,  $\beta = 3$ , q = 0.5

increases with increasing the coupling number N. A similar behavior happens for the micropolar parameter  $\beta$  (when:  $\phi = 0.5$ , x = 1,  $\alpha = 1$ , m = 1, N = 1, K = 0.5, q = 1) and the parameter  $\alpha$  (characterizes the microrotation on the solid surfaces, when:  $\phi = 0.5$ , x = 1, N = 1, K = 0.5,  $\beta = 3$ , q = 1). But the effect of the permeability parameter K on the velocity profile is illustrated in Figure 3. It is clear that velocity increases with increasing of K in the nominated region and then it decreases with increasing of K.



Figure 5. The microrotation  $^{W}$  against  $^{Y}$  for different values of K when:  $\phi = 0.5$ , x = 1,  $\alpha = 0$ ,  $\beta = 3$ , N = 0.5, q = 0.5.



Figure 6. The microrotation  $^{W}$  against  $^{Y}$  for different values of  $\beta_{\text{when:}} \phi = 0.5$ , x = 1,  $\alpha = 0$ , N = 0.5, K = 1.5,  $\alpha = 0$ , q = 0.5

Figure 4 explained the effect of coupling number N on microrotation velocity  ${}^{W}$ , it is observed that in the region  $0 \le y \le 0.6$  there is no effect of N on w (w has one behavior) and then  ${}^{W}$  decreases with increasing of N. The effect of the permeability parameter K on the microrotation velocity is illustrated in Figure 5. It is noted that  ${}^{W}$  decreases with increasing of K in the region  $0 \le y \le 1.25$  and subsequently this effect disappear and  ${}^{W}$  has one behavior. In Figure 6 it is clear that  ${}^{W}$  decreases with increasing of micropolar parameter  ${}^{\beta}$ , and its effect of the parameter  ${}^{\alpha}$  on  ${}^{W}$  is reflected as



Figure 7. The microrotation  $^{W}$  against  $^{y}$  for different values of  $\alpha$ when:  $\phi = 0.5$ , x = 1, N = 0.5, K = 1.5,  $\beta = 3$ , q = 0.5



Figure 8. The temperature distribution  $\theta$  against y for different values of  $R_n$  when:  $\phi = 0.5$ , x = 1,  $P_r = 5$ , G = 0.3.

shown in Figure 7.

Figures 8 explained the effects of radiation parameter  $R_n$  on the temperature distribution  $\theta$ , it is illustrated that  $\theta$  increases with increasing of it. The similar behavior occur with Prantdel number  $P_r$  (when:  $\phi = 0.5$ , x = 1,  $R_n = 5$ , G = 0.3) and generation parameter G (when:  $\phi = 0.5$ , x = 1,  $R_n = 5$ ,  $P_r = 5$ ). In Figure 9, the effect of  $R_n$  on the concentration distribution  $\phi$  is pointed out, it is observed that  $\phi$  decreases with increasing



Figure 9. The concentration  $\phi$  against y for different values of  $R_n$  when:  $\phi = 0.5$ , x = 1,  $P_r = 5$ , G = 0.3,  $S_c = 1.5$ ,  $S_r = 0.3$ .



Figure 10. The concentration  $\phi$  against y for different values of  $S_c$  when:  $\phi = 0.5$ , x = 1,  $R_n = 5$ ,  $P_r = 2o$ ,  $S_r = 0.3$ , G = 0.3.

of  $R_n$  and the similar behavior happen with  $P_r$  (when  $\phi = 0.5$ , x = 1,  $R_n = 5$ , G = 0.3,  $S_c = 1.5$ ,  $S_r = 0.3$ ). The effect of Schmit number  $S_c$  on the concentration distribution  $\phi$  is pointed out in Figure 10 and it is shown that  $\phi$  decreases with increasing of  $S_c$ . Figure 11 indicated the effect of Soret number  $S_r$  on  $\phi$ , it appeared that  $\phi$  decreases with increasing of it and the generation parameter G (when:  $\phi = 0.5$ , x = 1,  $R_n = 5$ ,  $P_r = 5$ ,  $S_c = 1.3$ ,  $S_r = 0.3$ ) has the same effect on  $\phi$ .



**Figure 11.** The concentration  $\phi$  against y for different values of

$$S_{r \text{ when:}} \phi = 0.5$$
,  $x = 1$ ,  $P_{r} = 5$ ,  $G = 0.3$ ,  
 $R_{n} = 5$ ,  $S_{c} = 1.3$ 

#### Conclusion

The problem of two dimensional peristaltic flow of a miropolar fluid through a symmetric channel with the effects of heat generation and radiation with heat and mass transfer has been investigated. The equations governing the fluid flow, subjected to a set of appropriate boundary conditions, have been solved analytically under the conditions of low Reynolds number and long wave length. The solutions of these equations are obtained as functions of the physical parameters of the problem, the effects of these parameters of the problem on these solutions have been shown graphically.

It appeared that the velocity profile increases with increasing of the parameters N,  $\beta$  and  $\alpha$  in the region  $0 \le y \le 0.8$ . The temperature distribution  $\theta$  increases with increasing of the parameters  $R_n$ ,  $P_r$  and G. The concentration distribution  $\phi$  decreases with increasing of  $R_n$  and  $P_r$  and decreases with increasing of the parameters  $S_c$ ,  $S_r$  and G.

#### REFERENCES

- Abo-Eldahab E, Barakat E, Nowar Kh (2012). Hall currents and heat transfer effects on peristaltic transport in a vertical asymmetric channel through a porous medium. Math. Probl. Eng. pp. 1-23.
- Ali N, Hayat T (2008). Peristaltic flow of a micropolar fluid in an asymmetric channel. J. Comput. Math. Appl. 55(4):589-608.
- Bayada G, Banhaoucha N (2008). Wall slip induced by a micropolar fluid. J. Eng. Math. 60:89-100.

- Devi G, Devanathan R (1975). Peristaltic motion of a micropolar fluid. Proc. Indian Acad. Sci. 81(A):149-163.
- Eldabe NTM (2001). Heat transfer of MHD Non-Newtonian Casson fluid between two rotating cylinders. Mech. Eng. 5(2):237-24.
- Eldabe NTM, El-Sayed MF, Ghaly AY, Sayed HM (2008). Mixed convective heat and mass transfer in a Non-Newtonian fluid at a peristaltic surface with temperature-dependent viscosity. Arch. Appl. Mech. 78:599-624.
- Eldabe NTM, Mohamed MAA (2002). Heat and mass transfer in hydromagnetic flow of the Non-Newtonian fluid with heat source over an accelerating surface through a porous medium. Chaos, Solitons Fractels. 13:907- 917.
- Eldabe NTM, Mohamed MAA, Hagag MA (2008). MHD flow and heat transfer of micropolar visco-elastic fluid between two parallel porous plats with time varing suction. J. Mech. Cont. Math. Sci. 3:217-233.
- El-Sayed MF, Eldabe NTM, Ghaly AY, Sayed HM (2011). Effects of chemical reaction, heat and mass transfer on non-Newtonian fluid flow through porous medium in a vertical peristaltic tube. Transp. Porous Med. 89:185-212.
- El-Shehawey EF, El-Dabe NT, El-ghzey EM, Ebaid A (2006). Peristaltic transport in an asymmetric channel through a porous medium. Appl. Math. Comput. 182:140-150.
- El-Shehawey EF, Husseny SZA (2000). Effects of porous boundaries on peristaltic transport through a porous medium. Acta Mech. 143:165-177.
- Eringen AC (1966). Theory of micropolar fluids. J. Math. Mech. 16:1-18.
- Eytan O, Jaffa AJ, Elad D (2001). Peristaltic flow in a tapered channel: Application to embryo transport within the uterine cavity. Med. Eng. Phys. 23:473-482.
- Fung YC, Yih CS (1968). Peristaltic transport. J. Appl. Mech. 35:669-675.
- Gharsseldien ZM (2003). On some problems in biofluidmechanics. PhD. dissertation, Math. Dept., Faculty of Science, Al-Azhar University. Egypt.
- Gharsseldien ZM, Mekheimer KS, Awad AS (2010). The influence of slippage on trapping and reflux limits with peristalsis through an asymmetric channel. Applied Bionics Biomech. 7(2):95-108.
- Hayat T, Ali N (2008). Effects of an endoscope on peristaltic flow of a micropolar fluid. Math. Comput. Model. 48:721-733.
- Hayat T, Ali N, Abbas Z (2007). Peristaltic flow of micropolar fluid in a channel with different wave forms. Phys. Lett. A. 370:331-344.
- Hayat T, Hina S (2010). The influence of wall properties on the MHD

Peristaltic flow of maxwell fluid with heat and mass transfer. Nonlinear Analysis: Real World Applications. 11:3155-3169.

Mahmoud MAA, Waheed SE (2012). MHD stagnation point flow of a

- micropolar fluid towards a moving surface with radiation. Meccanica. 47(5):1119-1130.
- Mekheimer KS (2003). Nonlinear peristaltic transport through a porous medium in an inclined planar channel. J. Porous Media. 6(3):189-201.
- Mekheimer KS, Abd Elmaboud Y (2008). The influence of a micropolar fluid on peristaltic transport in an annulus: application of the clot model. Appl.Bionics Biomech. 5(1):13-23.
- Mishra M, Rao AR (2003). Peristaltic transport of a Newtonian fluid in an asymmetric Channel. Z. angew. Math. Phys. 54:532-550.
- Muthu P, Ratnish KBV, Chandra P (2003). On the influence of wall properties in the peristaltic motion of micropolar fluid. ANZIAM J. 45:245-260.

- Muthu P, Ratnish KBV, Chandra P (2008). Peristaltic motion of micropolar fluid in circular cylindrical tubes: Effect of wall properties. Appld. Mathl. Model. 32:2019-2033.
- Nadeem S, Noreen SA (2009). Influnce of heat transfer on a peristaltic transport of Herschel-Bulkley fluid in a mon-uniform inclined tube. Commun. Nonlinear Sci. Numer. Simulat. 14:4100-4113.
- Nadeem S, Noreen SA, Bibi N, Ashiq S (2010). Influnce of heat and mass transfer on a peristaltic flow of a third order fluid in a diverging tube. Commun Nonlinear Sci. Numer. Simulat. 15:2916-2931.
- Srinivasacharya D, Mishra M, Rao AR (2003). Peristaltic pumping of a micropolar fluid in a tube. Acta. Mech. 161:165-178.
- Srivastava LM, Srivastava VP (1982). Peristaltic transport of a twolayered model of physiological fluid. J. Biomech. 15(4):257-265.

## APPENDIX

$$\begin{split} & \gamma_{1} = \frac{\sqrt{-\frac{\sqrt{K^{2}(N+2)^{2}\beta^{4} - 2K(N-2)^{2}\beta^{2} + (N-2)^{2} + K(N+2)\beta^{2} - N+2}{K(N-2)}}}{\sqrt{2}}, \\ & \gamma_{2} = 2\sqrt{\frac{\beta^{2}}{\sqrt{K^{2}(N+2)^{2}\beta^{4} - 2K(N-2)^{2}\beta^{2} + (N-2)^{2} + K(N+2)\beta^{2} - N+2}}, \\ & \gamma_{3} = \sqrt{\frac{3GR_{n}P_{r}}{-3R_{n} - 4}}, \quad L_{1} = n_{2} + n_{4} + n_{8}n_{9} - n_{11}, \quad L_{2} = n_{10}n_{12}, \quad L_{3} = n_{10}n_{13}, \quad L_{5} = n_{10}n_{14}, \\ & L_{4} = n_{3} + n_{5} + n_{6}, \\ & L_{6} = n_{10}n_{15}, \quad L_{7} = KN(n_{16} + n_{17} + n_{18}), \quad n_{1} = K(N\alpha - 2), \qquad n_{2} = 2q\gamma_{2}\sinh(h\gamma_{1})\cosh(h\gamma_{2}), \\ & n_{3} = h\gamma_{2}(n_{1}\gamma_{1}^{2} + 2)\sinh(h\gamma_{1})\cosh(h\gamma_{2}), \\ & n_{4} = -q\gamma_{1}(n_{1}\gamma_{2}^{2} + 2)\sinh(h\gamma_{2})\cosh(h\gamma_{1}), \qquad n_{7} = n_{1}\gamma_{2}^{2}\sinh(h\gamma_{2}), \\ & n_{8} = n_{1}\gamma_{1}^{2}\sinh(h\gamma_{2})(\sinh(h\gamma_{1}) - h\gamma_{1}\cosh(h\gamma_{1})), \\ & n_{8} = n_{1}\gamma_{1}^{2}\sinh(h\gamma_{1}), \quad n_{6} = \gamma_{1}\sinh(h\gamma_{2})(-n_{1}\gamma_{1}\sinh(h\gamma_{1}) - 2h\cosh(h\gamma_{1})), \qquad n_{9} = q\gamma_{2}\cosh(h\gamma_{2}), \\ & n_{10} = (h + q), \quad n_{11} = n_{7}\sinh(h\gamma_{1}) - n_{8}\sinh(h\gamma_{2}), \quad n_{12} = 2\sinh(h\gamma_{2}) + n_{7}, \\ & n_{13} = 2\sinh(h\gamma_{1}) + n_{8}, \quad n_{17} = n_{1}\gamma_{1}^{2}\sinh(h\gamma_{1})(\sinh(h\gamma_{2}) - h\gamma_{2}\cosh(h\gamma_{2})), \\ & n_{14} = (K\gamma_{1}^{2} - 1)(n_{1}\gamma_{2}^{2} + 2)\sinh(h\gamma_{2})\cos(h(\gamma_{1}), \quad n_{18} = -n_{1}\gamma_{2}\sinh(h\gamma_{2}) - 2h\cosh(h\gamma_{2}). \end{split}$$